Effect of laser in situ keratomileusis on vision analyzed using preoperative optical quality

Meritxell Vilaseca, PhD, Adenay Padilla, BSc, Juan C. Ondategui, MD, Montserrat Arjona, PhD, José L. Güell, MD, Jaume Pujol, PhD

PURPOSE: To evaluate the effect on vision of laser in situ keratomileusis (LASIK) based on preoperative optical quality.

SETTING: Universitat Politècnica de Catalunya, Terrassa, and Barcelona Institute of Ocular Microsurgery, Barcelona, Spain.

DESIGN: Comparative case series.

METHODS: The relative change in optical quality and visual acuity were evaluated in eyes that had LASIK for myopia. The optical quality was assessed before and 3 months after surgery using parameters provided by a double-pass system. Patients were classified into 4 groups by preoperative optical quality: low (Group 1), moderate (Group 2), high (Group 3), and very high (Group 4).

RESULTS: The study evaluated 25 patients (50 eyes). The optical quality parameters improved postoperatively in Group 1 and Group 2, with the improvement ranging from 15% to 21% and from 13% to 17%, respectively. The preoperative and postoperative optical quality in Group 3 was similar. The optical quality in Group 4 worsened significantly by percentages ranging from -20% to -26%. Although visual acuity had the same trend, there were no statistically significant changes.

CONCLUSION: The changes in optical quality after LASIK surgery depended on the patient's preoperative optical quality; visual acuity showed the same trend, although no change was significant.

Financial Disclosure: No author has a financial or proprietary interest in any material or method mentioned.

J Cataract Refract Surg 2010; 36:1945–1953 © 2010 ASCRS and ESCRS

Submitted: September 2, 2009. Final revision submitted: May 18, 2010. Accepted: May 18, 2010.

From the Centre for Sensors (Vilaseca, Arjona, Pujol), Instruments and Systems Development and the University Vision Centre (Padilla, Ondategui), Department of Optics and Optometry, Universitat Politècnica de Catalunya, Terrassa, and the Cornea-Refractive Surgery Unit (Güell), Barcelona Institute of Ocular Microsurgery, Barcelona, Spain.

Supported by the Spanish Ministry of Education and Science (grant DPI2008-06455-C02-01) and Visiometrics, S.L.

Corresponding author: Meritxell Vilaseca, PhD, Centre de Desenvolupament de Sensors, Instrumentació i Sistemes (CD6), Universitat Politècnica de Catalunya (UPC), Rambla Sant Nebridi 10, 08222 Terrassa, Barcelona, Spain. E-mail: mvilasec@oo.upc.edu. Laser in situ keratomileusis (LASIK)¹⁻⁵ is the most widely used ophthalmic surgical technique to correct refractive errors. The technique is mainly used to treat myopia,⁶⁻¹⁶ but can also be used to treat hyperopia¹⁷⁻¹⁹ and astigmatism.^{16,19,20} Laser in situ keratomileusis provides good results in most patients, with a reduced refractive error and acceptable vision postoperatively.²¹ Although LASIK outcomes are usually very satisfactory if the correct tools are applied, complications have been reported.^{3,22-26} These include infectious keratitis, dry eye, and diffuse lamellar keratitis. In addition, refractive complications, such as unexpected refractive outcomes, irregular astigmatism, decentering, visual aberrations, and loss of vision, can also occur. One advantage of LASIK is that most eyes can be retreated if necessary²⁷⁻²⁹; retreatment can resolve some refractive complications.

The follow-up clinical examination after LASIK is important. Many studies used subjective tests, such as standard visual acuity evaluations, and some used contrast sensitivity tests to assess postoperative LASIK patients.^{7,30–38} Today, it possible to objectively evaluate the eye's optical quality in clinical practice using aberrometers (usually based on the Hartmann-Shack wavefront sensor^{39,40} or laser ray tracing^{41,42}) and newer devices based on the double-pass technique.^{43,44}

In the past decade, aberrometers have become widely used for determining ocular aberrations in clinical ophthalmology and vision research. Thus, many studues have evaluated aberrations in normal eyes,^{45,46} in the elderly population,⁴⁷ and in eyes that have had refractive surgery, such as LASIK.^{41,42,48-53}

In the double-pass technique, the image of a pointsource object is recorded after reflection on the retina and a double pass through the ocular media. The technique has been shown to accurately estimate the eye's image quality. Although the clinical use of this technique is new, it has been used to analyze retinal image quality in the normal population as a function of age,⁵⁴ in contact lens wearers,^{55,56} in patients with monofocal^{57,58} or multifocal⁵⁹ IOLs, and in LASIK patients.⁵⁷

One study⁶⁰ recently compared the optical quality results of a double-pass device with those of a Hartmann-Shack wavefront sensor. The study found that the double-pass technique characterized the eye's optical quality, including the effect of monochromatic higher-order aberrations (HOAs), and especially intraocular scattering. However, the study's findings indicate that wavefront sensors may overestimate retinal image quality in eyes with prominent HOAs and scattered light. Furthermore, because the double-pass technique provides complete information on aberrations and intraocular scattering, it is useful for evaluating optical quality in patients who have ocular conditions such as cataract as well as in older eyes and eyes that have had refractive surgery.^{61–64}

In this study, we used a double-pass clinical system to analyze the changes in optical quality after LASIK. The changes in optical quality and the visual acuity were analyzed over time in patients with different preoperative optical quality.

PATIENTS AND METHODS

The study evaluated patients who had bilateral LASIK at the Barcelona Institute of Ocular Microsurgery. The LASIK was performed to correct moderate to high myopia (spherical equivalent 4.25 to 10.50 diopters [D]) in patients younger than 40 years. All patients provided written informed consent in accordance with the Declaration of Helsinki.

Inclusion criteria included stable myopia for the past year and a preoperative corrected distance visual acuity (CDVA) better than 20/30. The last criterion was applied because in some cases, a CDVA worse than 20/20 might be the result of a small degree of amblyopia.

Surgical Technique

The same surgeon (J.L.G.) performed all LASIK procedures using an MEL 80 excimer laser with the Aberration Smart Ablation optimized profile (Carl Zeiss Meditec), a 6.2 mm optical zone, and a standard 8.2 mm transition zone. The ablation profile corresponds to a wavefrontoptimized treatment that mainly takes into account final asphericity to reduce the induction of spherical aberration. The flap was created with an Amadeus microkeratome (Ziemer Group AG) with a 140 μ m plate and 9.0 mm diameter.

Postoperatively, patients received tobramycin-dexamethasone (TobraDex) and timolol maleate 0.5% (Cusimolol) 4 times a day and dexamethasone sodium phosphate –chloramphenicol ointment (De Icol) at bedtime for 2 weeks and then tapered over 10 days. Patients were instructed to use artificial tears at least 5 times a day for 2 months.

Patient Evaluation

Optical quality was assessed preoperatively and 3 months postoperatively using a commercially available double-pass system (Optical Quality Analysis System, Visiometrics S.L.). Artificial tears were instilled immediately before each measurement. The refractive error was corrected during measurements to obtain the best retinal image; the spherical refractive error was automatically corrected by the doublepass system, and astigmatism was corrected with an external



Figure 1. The double-pass experimental setup (BS1 and BS2 = beam splitters 1 and 2, respectively; CCD1 and CCD2 = charge-coupled-device cameras 1 and 2, respectively; DF = dichroic filter; EP = entrance pupil; ExP = exit pupil; FT = fixation test; IL = infrared light-emitting diode; L1, L2, L3, L4, and L5 = lenses 1, 2, 3, 4, and 5, respectively; LD = laser diode; M1, M2, M3, and M4 = mirrors 2, 2, 3, and 4, respectively).

2 versus 3

2 versus 4

3 versus 4

(Student t test)

Table 1. Preoperative refractive error by group.			
Group	Sphere (D)	Cylinder (D)	SE (D)
1 (6 eyes)			
Mean \pm SD	6.50 ± 1.33	1.36 ± 1.00	7.21 ± 1.83
Range	5.00 to 9.00	0.25 to 3.00	5.00 to 10.50
2 (15 eyes)			
Mean \pm SD	6.01 ± 1.16	1.08 ± 0.89	6.55 ± 1.61
Range	4.25 to 7.75	0.00 to 3.00	4.25 to 9.25
3 (18 eyes)			
Mean \pm SD	5.66 ± 1.04	0.68 ± 0.55	5.96 ± 1.28
Range	4.25 to 7.75	0.00 to 2.00	4.25 to 8.75
4 (11 eyes)			
Mean \pm SD	5.73 ± 0.74	0.69 ± 0.55	6.08 ± 1.01
Range	4.50 to 7.50	0.00 to 2.00	4.50 to 8.50
SE = spherical equations for the second se	SE = spherical equivalent		

lens. Because the optical quality of the external lenses is much higher than the optical quality of the eye (in general, this is accomplished by other optical elements, such as intraocular lenses⁶⁵), the final optical quality measurement is not affected by the external lenses.

Figure 1 shows a diagram of the double-pass system. Because of its asymmetric configuration, asymmetrical aberrations in retinal images can be captured. The instrument 44,60 records the retinal image corresponding to a point-source object in near-infrared light, which consists of a laser diode (wavelength 780 nm) coupled to an optical fiber. The image is captured after reflection on the retina and a double pass through the ocular media. Near-infrared light is used because it for patient comfort and it provides retinal image quality estimates comparable to those obtained with visible light.66 A motorized optometer consisting of 2 lenses with a 100 mm focal length and 2 mirrors measures the patient's defocus correction. An infrared video camera with a pixel size of 8.4 µm records the double-pass images after the light is reflected on the retina and on a beam splitter. Pupil alignment is controlled with an additional camera. A fixation test is used to help patients fixate during measurements. The

Table 3. Three-month postoperative refractive error by group.			
Group	Sphere (D)	Cylinder (D)	SE (D)
1 (6 eyes)			
Mean \pm SD	-0.50 ± 0.58	-0.71 ± 0.39	-0.86 ± 0.77
Range	-1.75 to 0.00	-1.25 to 0.00	-2.25 to 0.00
2 (15 eyes)			
Mean \pm SD	-0.30 ± 0.29	-0.46 ± 0.47	-0.53 ± 0.53
Range	-0.75 to 0.25	-1.25 to 0.00	-1.25 to 0.25
3 (18 eyes)			
Mean \pm SD	-0.20 ± 0.40	-0.23 ± 0.34	-0.31 ± 0.57
Range	-1.25 to 0.50	-1.25 to 0.00	-1.75 to 0.50
4 (11 eyes)			
Mean \pm SD	-0.13 ± 0.30	-0.42 ± 0.43	-0.34 ± 0.51
Range	-0.75 to 0.25	-1.25 to 0.00	-1.25 to 0.25
SE = spherical equivalent			

Table 2. Statistical sphere and cylinder	l comparison between gro er in the 4 groups.	oups of preoperative
	P \	/alue*
Group	Sphere	Cylinder
1 versus 2	.333	.488
1 versus 3	.110	.049
1 vorene 4	120	052

.289

.411

.796

entrance pupil has a fixed diameter of 2.0 mm. The instrument has an artificial and variable exit pupil controlled by a diaphragm wheel whose image is formed on the patient's natural pupil plane. In this study, optical quality measurements were performed using a standard pupil diameter of 4.0 mm.

Optical quality parameters⁶⁷ related to the monochromatic averaged modular transfer function (MTF) profile corresponding to all radial directions were assessed; these parameters were directly computed by the double-pass system. The MTF profile contains all information on the eye's optical quality with regard to monochromatic aberrations and scattered light. One optical quality parameter assessed was the Strehl ratio,68 which is often computed in the frequency domain as the ratio between the volumes under the MTF curve of the measured eye and that of the aberration-free eye.^{69,70} The double-pass computes the Strehl ratio in 2 dimensions (2D Strehl ratio) as the ratio between the areas under the MTF curve of the measured eye and that of the aberration-free eye, which is also accepted in the literature⁶⁹ and is related to a smaller computational cost in time, which makes this approach more suitable for the clinical practice.

The other optical quality parameters (called OV) represent normalized values for 3 spatial frequencies that correspond to MTF values. The values describe the optical quality under 3 contrast conditions (100%, 20%, 9%). Specifically, the 100% value is directly related to the MTF cutoff frequency; that is, the MTF cutoff frequency divided by 30 cycles per degree (cpd). It is normally given that a cutoff frequency of 30 cpd in contrast sensitivity function corresponds to a visual acuity

	P V	'alue*
Group	Sphere	Cylinder
1 versus 2	.239	.221
1 versus 3	.125	.051
1 versus 4	.058	.129
2 versus 3	.349	.064
2 versus 4	.069	.679
3 versus 4	.472	.172

.080

.136

.665

of 20/20.⁷¹ In the double-pass system, the MTF cutoff is calculated as that corresponding to a MTF value of 0.01 because in the MTF profile computed from the real recorded double-pass image, there is some background noise. The 20% and 9% values are computed in the same way from smaller frequencies linked to MTF values of 0.05 and 0.10, respectively, that maintain the proportion of contrasts 20% and 9%, respectively. These frequencies are also normalized so that the values obtained are comparable to standard decimal visual acuity values.⁵⁷ Values higher than 1.00 are associated with high optical quality.

The eyes were divided into 4 groups based on the preoperative 100% values as follows: low optical quality (100% value ≤ 0.6 ; Group 1), moderate optical quality (100% value >0.6 to ≤ 0.9 ; Group 2), high optical quality (100% value >0.9 to ≤ 1.2 ; Group 3), and very high optical quality (100% value 1.2; Group 4).

The decimal CDVA was assessed with a standard Snellen test preoperatively and 3 months postoperatively. The uncorrected distance visual acuity (UDVA) was measured at 3 months.

Statistical Analysis

Statistical analysis was performed using SPSS for Windows software (version 17.0, SPSS, Inc.). The results were expressed as the mean \pm the standard deviation. Statistically significant differences in mean values were determined using the Student *t* test and paired *t* test. A *P* value less than 0.05 was considered statistically significant.

RESULTS

The study evaluated 50 eyes of 25 patients. There were no postoperative complications.

Refractive Error

Table 1 shows the number of eyes and preoperative refraction in each of the 4 groups. The degree of myopia was similar between the groups. Table 2 gives the *P* values for between-group comparisons of sphere and cylinder. Although there were no statistically significant differences, the differences in cylinder between Group 1 and Group 3 and between Group 1 and Group 4 approached statistical significance.

Table 3 shows the mean 3-month postoperative refractive error by group. There were no statistically significant differences between the groups in sphere or cylinder (Table 4).

Optical Quality

Figure 2 shows representative retinal images recorded preoperatively and 3 months postoperatively using the double-pass system. The images correspond to 4 patients, 1 in each optical quality group.

Figure 3 shows the mean preoperative and postoperative MTF profiles by optical quality group. The MTF for an aberration-free eye with a 4.0 mm size is also plotted. Table 5 shows the mean optical quality parameters preoperatively and 3 months postoperatively by optical quality group. In Group 1, the change from preoperatively to postoperatively was statistically significant for the 2D Strehl ratio (P = .042) and for all 3 contrasts (100%, P = .049; 20%, P = .049; and 9%, P = .083; paired *t* test).

Preoperative

Postoperative



Group 1



Group 2



Group 3



Figure 2. Representative retinal images.



Figure 3. Mean preoperative and postoperative MTF results by group. The MTF corresponding to an aberration-free eye with a 4.0 mm pupil is also plotted (cpd = cycles per degree; MTF = modulation transfer function).

In Group 2, the change was statistically significant for the 2D Strehl ratio (P = .069) and for all 3 contrasts (100%, P = .009; 20%, P = .008; and 9%, P = .049; paired *t* test).

In Group 3, there were no statistically significant changes (2D Strehl ratio, P = .497; 100% contrast, P = .107; 20% contrast, P = .555; and 9% contrast, P = .904; paired *t* test).

In Group 4, the change was highly statistically significant for the 2D Strehl ratio (P = .0005) and for all 3 contrasts (100%, P < .0001; 20%, P < .0001; and 9%, P < .0005; paired *t* test).

Visual Acuity

Table 6 shows the mean preoperative CDVA and the postoperative CDVA and UDVA by group. Although visual acuity had the same trend as the optical quality parameters, there were no statistically significant changes in CDVA from preoperatively to postoperatively (Group 1, P = .104; Group 2, P = .054; Group 3, P = .512; and Group 4, P = .507; paired *t* test).

Figure 4 shows the percentage of improvement in or worsening of the optical quality parameters and the CDVA, calculated as follows: Percentage = [(Postoperative/Preoperative) parameter -1] × 100.

DISCUSSION

As seen in our study, some eyes have better preoperative optical quality than others, possibly because of a combination of factors including the degree of ametropia, keratometry values, degree of irregular astigmatism, and corneal and intraocular HOAs. In our study, the spot size of the retinal images decreased after the LASIK in eyes with low optical quality (Group A) or moderate optical quality (Group B) preoperatively. In eyes with high optical quality (Group C) and very high optical quality (Group D) preoperatively, the spot size of the retinal images increased after LASIK. The same trend was seen in the mean MTF profiles. The mean MTF improved after LASIK in Group 1 and Group 2 and worsened in Group 3 and Group 4.

The 2D Strehl ratio calculated by the double-pass system evolved differently over time depending on the optical quality group. The ratio increased postoperatively in Group 1 and Group 2 and decreased in Group 3 and Group 4, especially the Group 4. Group 1 and Group 2 had an improvement of 21% and 13%, respectively, whereas Group 3 and Group 4 had a decrease of 4% and 20%, respectively. The differences were statistically significant in Group 1 and Group 4.

	Mean \pm SD			
			Contrast	
Group/Exam	Strehl 2D	100%	20%	9%
Group 1				
Preop	0.099 ± 0.014	0.47 ± 0.04	0.46 ± 0.07	0.48 ± 0.10
3 mo postop	0.120 ± 0.016	0.56 ± 0.12	0.55 ± 0.11	0.55 ± 0.10
Group 2				
Preop	0.135 ± 0.026	0.74 ± 0.09	0.72 ± 0.11	0.74 ± 0.16
3 mo postop	0.152 ± 0.017	0.85 ± 0.10	0.84 ± 0.10	0.84 ± 0.12
Group 3				
Preop	0.163 ± 0.024	1.06 ± 0.06	1.01 ± 0.10	0.95 ± 0.15
3 mo postop	0.157 ± 0.030	0.98 ± 0.15	0.97 ± 0.16	0.95 ± 0.19
Group 4				
Preop	0.227 ± 0.022	1.41 ± 0.08	1.37 ± 0.13	1.34 ± 0.16
3 mo postop	0.181 ± 0.025	1.04 ± 0.14	1.01 ± 0.15	1.04 ± 0.16

The values of all 3 contrast values calculated by the double-pass system showed similar behavior and correlated well with the Strehl parameter; their evolution also varied by group. The mean 100% value increased postoperatively in Group 1 and Group 2 and decreased in Group 3 and Group 4, especially in the latter group. The mean improvement in the 100% value was 19% in Group 1 and 15% in Group 2. In contrast, the mean optical quality decreased by 7% in Group 3 and by approximately 26% in Group 4. The change was statistically significant in all groups except Group 3, in which the change was small.

	Mean \pm SD		
Group/Exam	CDVA	UDVA	
Group 1			
Preop	0.82 ± 0.07	_	
3 mo postop	0.83 ± 0.13	0.74 ± 0.13	
Group 2			
Preop	0.84 ± 0.09	_	
3 mo postop	0.85 ± 0.10	0.77 ± 0.12	
Group 3			
Preop	0.90 ± 0.08	—	
3 mo postop	0.89 ± 0.10	0.84 ± 0.10	
Group 4			
Preop	0.91 ± 0.07	—	
3 mo postop	0.89 ± 0.15	0.78 ± 0.13	

A similar evolution was seen for the 20% and 9% values. The 20% value improved by 20% and 17% in Group 1 and Group 2, respectively, and decreased by 4% and 26% in Group 3 and Group 4, respectively. Again, the only group that did not have a statistically significant change was Group 3. The 9% value improved by 15% in Group 1 and 14% in Group 2 and decreased by 22% in Group 4. The mean 9% value in Group 3 remained unchanged. The changes in the 9% value was statistically significant in Group 2 and Group 4.

The CDVA also changed over time in some groups, although it not as much as the 2D Strehl ratio and the 3 contrast values. This may be attributed to retinal or neural factors, which are not included in the optical



Figure 4. Percentage improvement or worsening in mean optical quality and CDVA by group (CDVA = corrected distance visual acuity; Strehl D = Strehl ratio in 2 dimensions).

quality parameters. The CDVA improved by 1% in Group 1 and in Group 2 and was worse by 1% in Group 3 and 2% in Group 4. None of the changes was statistically significant.

The changes in the optical quality parameters show that the patients with low or moderate optical quality before surgery generally had a relative improvement in optical quality after LASIK. Patients with high optical quality before surgery had similar optical quality after LASIK. Finally, patients with very high optical quality before surgery had a decline in optical quality after surgery. The reason most eyes with low to moderate optical quality limited improvement in optical quality after LASIK might be a result of the small change in the asphericity and precise correction of the ametropic error. In some cases, the surgery may have compensated for a portion of the irregular astigmatism. The trend was not remarkable for CDVA. The objective optical quality parameters proved more useful in this case because they allowed better discrimination of the results in the different groups of patients.

Our study shows that the double-pass technique can be useful in determining the influence of refractive surgical procedures on the optical quality of the eye through a comparison of preoperative and postoperative images, including HOAs and intraocular scattering individually and over time. Furthermore, the changes in optical quality parameters probably explain why some patients with very high optical quality before surgery report being unsatisfied with their postoperative vision despite a good refractive result.

REFERENCES

- Schwiegerling J. LASIK and beyond. Opt Photonics News 2002; 13:30–33
- Barraquer JI. The history and evolution of keratomileusis. Int Ophthalmol Clin 1996; 36(4):1–7
- Buratto L, Ferrari M. Indications, techniques, results, limits, and complications of laser in situ keratomileusis. Curr Opin Ophthalmol 1997; 8(4):59–66
- Farah SG, Azar DT, Gurdal C, Wong J. Laser in situ keratomileusis: literature review of a developing technique. J Cataract Refract Surg 1998; 24:989–1006
- Pallikaris IG, Papatzanaki ME, Stathi EZ, Frenschock O, Georgiadis A. Laser in situ keratomileusis. Lasers Surg Med 1990; 10:463–468
- Güell JL, Muller A. Laser in situ keratomileusis (LASIK) for myopia from -7 to -18 diopters. J Refract Surg 1996; 12:222–228
- Marinho A, Pinto MC, Pinto R, Vaz F, Neves MC. LASIK for high myopia: one year experience. Ophthalmic Surg Lasers 1996; 27:S517–S520
- Bas AM, Onnis R. Excimer laser in situ keratomileusis for myopia. J Refract Surg 1995; 11:S229–S233
- Chayet AS, Assil KK, Montes M, Espinosa-Lagana M, Castellanos A, Tsioulias G. Regression and its mechanisms after laser in situ keratomileusis in moderate and high myopia. Ophthalmology 1998; 105:1194–1199. Available at: http://download.

journals.elsevierhealth.com/pdfs/journals/0161-6420/PIIS016164 2098970208.pdf. Accessed July 3, 2010

- Pallikaris IG, Siganos DS. Laser in situ keratomileusis to treat myopia: early experience. J Cataract Refract Surg 1997; 23:39–49
- 11. Yoo SH, Azar DT. Laser in situ keratomileusis for the treatment of myopia. Int Ophthalmol Clin 1999; 39(1):37–44
- Alió JL, Muftuoglu O, Ortiz D, Pérez-Santonja JJ, Artola A, Ayala MJ, Garcia MJ, Castro de Luna G. Ten-year follow-up of laser in situ keratomileusis for myopia of up to -10 diopters. Am J Ophthalmol 2008; 145:46-54
- Bahar I, Levinger S, Kremer I. Wavefront-guided LASIK for myopia with the Technolas 217z: results at 3 years. J Refract Surg 2007; 23:586–590; editor's note, 591
- El Danasoury MA, El Maghraby A, Klyce SD, Mehrez K. Comparison of photorefractive keratectomy with excimer laser in situ keratomileusis in correcting low myopia from -2.00 to -5.50 diopters; a randomized study. Ophthalmology 1999; 106:411-420. discussion by JH Talamo, 420-421. Available at: http://download.journals.elsevierhealth.com/pdfs/journals/0161-6420/PIIS016164209900842.pdf. Accessed July 3, 2010
- Lavery F. Laser in situ keratomileusis for myopia. J Refract Surg 1998; 14:S177–S178
- Sugar A, Rapuano CJ, Culbertson WW, Huang D, Varley GA, Agapitos PJ, de Luise VP, Koch DD. Laser in situ keratomileusis for myopia and astigmatism: safety and efficacy; a report by the American Academy of Ophthalmology (Ophthalmic Technology Assessment). Ophthalmology 2002; 109:175–187. Available at: http://download.journals.elsevierhealth.com/pdfs/journals/0161 -6420/PIIS0161642001009666.pdf. Accessed July 3, 2010
- Barraquer JI. Results of hypermetropic keratomileusis, 1980-1981. Int Ophthalmol Clin 1983; 23(3):25–44
- Göker S, Er H, Kahvecioglu C. Laser in situ keratomileusis to correct hyperopia from +4.25 to +8.00 diopters. J Refract Surg 1998; 14:26–30
- Ibrahim O. Laser in situ keratomileusis for hyperopia and hyperopic astigmatism. J Refract Surg 1998; 14:S179– S182
- Argento C, Fernández Mendy J, Cosentino MJ. Laser in situ keratomileusis versus arcuate keratotomy to treat astigmatism. J Cataract Refract Surg 1999; 25:374–382
- Bailey MD, Mitchell GL, Dhaliwal DK, Boxer Wachler BS, Zadnik K. Patient satisfaction and visual symptoms after laser in situ keratomileusis. Ophthalmology 2003; 110:1371–1378. Available at: http://download.journals.elsevierhealth.com/pdfs/ journals/0161-6420/PIIS016164200300455X.pdf. Accessed July 3, 2010
- 22. Melki SA, Azar DT. LASIK complications: etiology, management, and prevention. Surv Ophthalmol 2001; 46:95–116
- Davidorf JM, Zaldivar R, Oscherow S. Results and complications of laser in situ keratomileusis by experienced surgeons. J Refract Surg 1998; 14:114–122
- Davis EA, Hardten DR, Lindstrom RL. LASIK complications. Int Ophthalmol Clin 2000; 40(3):67–75
- Iskander NG, Peters NT, Anderson Penno E, Gimbel HV. Postoperative complications in laser in situ keratomileusis. Curr Opin Ophthalmol 2000; 11:273–279
- Stulting RD, Carr JD, Thompson KP, Waring GO III, Wiley WM, Walker JG. Complications of laser in situ keratomileusis for the correction of myopia. Ophthalmology 1999; 106:13–20. Available at: http://download.journals.elsevierhealth.com/pdfs/journals/ 0161-6420/PIIS0161642099900003.pdf. Accessed July 3, 2010
- Castanera J, Serra A, Rios C. Wavefront-guided ablation with Bausch and Lomb Zyoptix for retreatments after laser in situ keratomileusis for myopia. J Refract Surg 2004; 20:439–443

- Febbraro J-L, Buzard KA, Friedlander MH. Reoperations after myopic laser in situ keratomileusis. J Cataract Refract Surg 2000; 26:41–48
- Netto MV, Wilson SE. Flap lift for LASIK retreatment in eyes with myopia. Ophthalmology 2004; 111:1362–1367. Available at: http://download.journals.elsevierhealth.com/pdfs/journals/ 0161-6420/PIIS016164200400171X.pdf. Accessed July 3, 2010
- Malecaze FJ, Hulin H, Bierer P, Fournié P, Grandjean H, Thalamas C, Guell JL. A randomized paired eye comparison of two techniques for treating moderately high myopia; LASIK and Artisan phakic lens. Ophthalmology 2002; 109:1622– 1630. Available at: http://download.journals.elsevierhealth. com/pdfs/journals/0161-6420/PIIS0161642002011648.pdf. Accessed July 3, 2010
- Kim TW, Wee WR, Lee JH, Kim MK. Contrast sensitivity after LASIK, LASEK, and wavefront-guided LASEK with the VISX S4 laser. J Refract Surg 2007; 23:355–361
- Bailey MD, Olson MD, Bullimore MA, Jones L, Maloney RK. The effect of LASIK on best-corrected high- and low-contrast visual acuity. Optom Vis Sci 2004; 81:362–368
- Mutyala S, McDonald MB, Scheinblum KA, Ostrick MD, Brint SF, Thompson H. Contrast sensitivity evaluation after laser in situ keratomileusis. Ophthalmology 2000; 107:1864–1867. Available at: http://download.journals.elsevierhealth.com/pdfs/journals/ 0161-6420/PIIS0161642000003559.pdf. Accessed July 3, 2010
- Pérez-Santonja JJ, Sakla HF, Alió JL. Contrast sensitivity after laser in situ keratomileusis. J Cataract Refract Surg 1998; 24:183–189
- Hoffman RS, Packer M, Fine IH. Contrast sensitivity and laser in situ keratomileusis. Int Ophthalmol Clin 2003; 43(2):93–100
- Montés-Micó R, Charman WN. Choice of spatial frequency for contrast sensitivity evaluation after refractive surgery. J Refract Surg 2001; 17:646–651
- Nakamura K, Bissen-Miyajima H, Toda I, Hori Y, Tsubota K. Effect of laser in situ keratomileusis correction on contrast visual acuity. J Cataract Refract Surg 2001; 27:357–361
- Pesudovs K, Hazel CA, Doran RML, Elliott DB. The usefulness of Vistech and FACT contrast sensitivity charts for cataract and refractive surgery outcomes research. Br J Ophthalmol 2004; 88:11–16. Available at: http://www.ncbi.nlm.nih.gov/pmc/articles/ PMC1771933/pdf/bjo08800011.pdf. Accessed July 1, 2010
- Prieto PM, Vargas-Martín F, Goelz S, Artal P. Analysis of the performance of the Hartmann-Shack sensor in the human eye. J Opt Soc Am A Opt Image Sci Vis 2000; 17:1388–1398
- Liang J, Grimm B, Goelz S, Bille JF. Objective measurement of wave aberrations of the human eye with the use of a Hartmann– Shack wave-front sensor. J Opt Soc Am A Opt Image Sci Vis 1994; 11:1949–1957
- Moreno-Barriuso E, Merayo Lloves J, Marcos S, Navarro R, Llorente L, Barbero S. Ocular aberrations before and after myopic corneal refractive surgery: LASIK-induced changes measured with laser ray tracing. Invest Ophthalmol Vis Sci 2001; 42:1396–1403. Available at: http://www.iovs.org/cgi/reprint/42/ 6/1396.pdf. Accessed July 1, 2010
- 42. Marcos S. Aberrations and visual performance following standard laser vision correction. J Refract Surg 2001; 17:S596–S601
- Santamaría J, Artal P, Bescós J. Determination of the pointspread function of human eyes using a hybrid optical-digital method. J Opt Soc Am A 1987; 4:1109–1114
- Güell JL, Pujol J, Arjona M, Diaz-Douton F, Artal P. Optical Quality Analysis System: instrument for objective clinical evaluation of ocular optical quality. J Cataract Refract Surg 2004; 30:1598–1599
- Castejón-Mochón JF, López-Gil N, Benito A, Artal P. Ocular wave-front aberration statistics in a normal young population. Vision Res 2002; 42:1611–1617

- Porter J, Guirao A, Cox IG, Williams DR. Monochromatic aberrations of the human eye in a large population. J Opt Soc Am A Opt Image Sci Vis 2001; 18:1793–1803
- Artal P, Berrio E, Guirao A, Piers P. Contribution of the cornea and internal surfaces to the change of ocular aberrations with age. J Opt Soc Am A Opt Image Sci Vis 2002; 19:137–143
- Lee HW, Park SC, Park DW, Cheng T-Y, Cheng E-S. Comparative analysis of postoperative changes in higher order aberrations following LASIK and laser thermal keratoplasty [letter]. J Refract Surg 2007; 23:224–225
- Yoon G, MacRae S, Williams DR, Cox IG. Causes of spherical aberration induced by laser refractive surgery. J Cataract Refract Surg 2005; 31:127–135
- Subbaram MV, MacRae SM, Slade SG, Durrie DS. Customized LASIK treatment for myopia: relationship between preoperative higher order aberrations and refractive outcome. J Refract Surg 2006; 22:746–753
- Yamane N, Miyata K, Samejima T, Hiraoka T, Kiuchi T, Okamoto F, Hirohara Y, Mihashi T, Oshika T. Ocular higherorder aberrations and contrast sensitivity after conventional laser in situ keratomileusis. Invest Ophthalmol Vis Sci 2004; 45:3986–3990. Available at: http://www.iovs.org/cgi/reprint/45/ 11/3986. Accessed July 1, 2010
- Chandhrasri S, Knorz MC. Comparison of higher order aberrations and contrast sensitivity after LASIK, Verisyse phakic IOL, and Array multifocal IOL. J Refract Surg 2006; 22:231–236
- Oshika T, Klyce SD, Applegate RA, Howland HC, El Danasoury MA. Comparison of corneal wavefront aberrations after photorefractive keratectomy and laser in situ keratomileusis. Am J Ophthalmol 1999; 127:1–7
- 54. Guirao A, González C, Redondo M, Geraghty E, Norrby S, Artal P. Average optical performance of the human eye as a function of age in a normal population. Invest Ophthalmol Vis Sci 1999; 40:203–213. Available at: http://www.iovs.org/cgi/reprint/ 40/1/203.pdf. Accessed July 1, 2010
- Pujol J, Gispets J, Arjona M. Optical performance in eyes wearing two multifocal contact lenses design. Ophthalmic Physiol Opt 2003; 23:347–360
- Gispets J, Arjona M, Pujol J. Image quality in wearers of a centre distance concentric design bifocal contact lens. Ophthalmic Physiol Opt 2002; 22:221–233
- 57. Vilaseca M, Padilla A, Pujol J, Ondategui JC, Artal P, Güell JL. Optical quality one month after Verisyse and Veriflex phakic IOL implantation and Zeiss MEL 80 LASIK for myopia from 5.00 to 16.50 diopters. J Refract Surg 2009; 25:689–698
- Guirao A, Redondo M, Geraghty E, Piers P, Norrby S, Artal P. Corneal optical aberrations and retinal image quality in patients in whom monofocal intraocular lenses were implanted. Arch Ophthalmol 2002; 120:1143–1151
- Artal P, Marcos S, Navarro R, Miranda I, Ferro M. Through focus image quality of eyes implanted with monofocal and multifocal intraocular lenses. Opt Eng 1995; 34:772–779. Available at: http://www. vision.csic.es/Publications/Articles/Through%20focus%20image% 20quality%20of%20eyes%20implanted%20with%20monofocal% 20and%20multifocal%20intraocular%20lenses.pdf. Accessed July 3, 2010
- 60. Díaz-Doutón F, Benito A, Pujol J, Arjona M, Güell JL, Artal P. Comparison of the retinal image quality obtained with a Hartmann-Shack sensor and a double-pass instrument. Invest Ophthalmol Vis Sci 2006; 47:1710–1716. Available at: www.iovs. org/cgi/reprint/47/4/1710.pdf. Accessed July 1, 2010
- Fan-Paul NI, Li J, Sullivan Miller J, Florakis GJ. Night vision disturbances after corneal refractive surgery. Surv Ophthalmol 2002; 47:533–546

- El Danasoury MA. Prospective bilateral study of night glare after laser in situ keratomileusis with single zone and transition zone ablation. J Refract Surg 1998; 14:512–516
- Jain S, Khoury JM, Chamon W, Azar DT. Corneal light scattering after laser in situ keratomileusis and photorefractive keratectomy. Am J Ophthalmol 1995; 120:532–534
- Holladay JT, Dudeja DR, Chang J. Functional vision and corneal changes after laser in situ keratomileusis determined by contrast sensitivity, glare testing, and corneal topography. J Cataract Refract Surg 1999; 25:663–669
- Vilaseca M, Arjona M, Pujol J, Issolio L, Güell JL. Optical quality of foldable monofocal intraocular lenses before and after injection; comparative evaluation using a double-pass system. J Cataract Refract Surg 2009; 35:1415–1423
- López-Gil N, Artal P. Comparison of double-pass estimates of the retinal-image quality obtained with green and near-infrared light. J Opt Soc Am A 1997; 14:961–971
- Saad A, Saab M, Gatinel D. Repeatability of measurements with a double-pass system. J Cataract Refract Surg 2010; 36:28–33
- Born M, Wolf E. Principles of Optics; Electromagnetic Theory of Propagation, Interference and Diffraction of Light, 7th ed. Cambridge, UK, Cambridge University Press, 1999

- Thibos LN, Hong X, Bradley A, Applegate RA. Accuracy and precision of objective refraction from wavefront aberrations. J Vis 2004; 4(4):329–351. Available at: http://www.journalofvision. org/content/4/4/9.full.pdf + html. Accessed July 1, 2010
- Navarro R, Artal P, Williams DR. Modulation transfer of the human eye as a function of retinal eccentricity. J Opt Soc Am A 1993; 10:201–212
- 71. Schwartz SH. Visual Perception; A Clinical Orientation, 2nd ed. New York, NY, McGraw Hill, 1999



First author: Meritxell Vilaseca, PhD

Centre for Sensors, Instruments and Systems Development, Department of Optics and Optometry, Universitat Politècnica de Catalunya, Terrassa, Spain